Layered Double Hydroxides as a Drug Delivery Vehicle for S-Allyl-Mercapto-Cysteine (SAMC)

Ivan Vito Ferrari, Riccardo Narducci, Giuseppe Prestopino, Ferdinando Costantino, Alessio Mattoccia, Lina Di Giamberardino, Morena Nocchetti, Maria Luisa Di Vona, Annalisa Paolone, Marzia Bini, Riccardo Pezzilli, Ilaria Borromeo, Simone Beninati and Pier Gianni Medaglia

Abstract: The intercalations of anionic molecules and drugs in layered double hydroxides (LDHs) have been intensively investigated in recent years. Due to their properties, such as versatility in chemical composition, good biocompatibility, high density and protection of loaded drugs, LDHs seem very promising nanosized systems for drug delivery. In this work, we report the intercalation of S-allyl-mercaptop-cysteine (SAMC), which is a component of garlic that is well-known for its anti-tumor properties, inside ZnAl-LDH (hereafter LDH) nanostructured crystals. In order to investigate the efficacy of the intercalation and drug delivery of SAMC, the intercalated compounds were characterized using X-ray powder diffraction (XRD), Fourier-transform infrared spectroscopy (FT-IR) and scanning electron microscopy (SEM). The increase in the interlayer distance of LDH from 8.9 Å, typical of the nitrate phase, to 13.9 Å indicated the intercalation of SAMC, which was also confirmed using FT-IR spectra. Indeed, compared to that of the pristine LDH precursor, the spectrum of LDH-SAMC was richly structured in the fingerprint region below 1300 cm⁻¹, whose peaks corresponded to those of the functional groups in the SAMC molecular anion. The LDH-SAMC empirical formula, obtained from UV-Vis spectrophotometry and thermogravimetric analysis, was [Zn₀.₆₇Al₀.₃₃(OH)₂]SAMC₀.₁₅(NO₃₀.₃₈·0.₆H₂O). The morphology of the sample was investigated using SEM: LDH-SAMC exhibited a more irregular size and shape of the flake-like crystals in comparison with the pristine LDH, with a reduction in the average crystallite size from 3 μm to about 2 μm. In vitro drug release studies were performed in a phosphate buffer solution at pH 7.2 and 37 °C and were analyzed using UV-Vis spectrophotometry. The SAMC release from LDH-SAMC was initially characterized by a burst effect in the first four hours, during which, 32% of the SAMC is released. Subsequently, the release percentage increased at a slower rate until 42% after 48 h; then it stabilized at 43% and remained constant for the remaining period of the investigation. The LDH-SAMC complex that was developed in this study showed the improved efficacy of the action of SAMC in reducing the invasive capacity of a human hepatoma cell line.

Keywords: ZnAl-LDH; intercalation compounds; S-allyl-mercaptop-cysteine (SAMC); drug delivery; cancer; hepatoma; antitumor garlic derivative molecules
1. Introduction

Chemotherapy with cytotoxic drugs is widely used for the treatment of cancer patients. However, the use of these drugs has shown the development of resistance of cancer cells to treatment with these anticancer agents. The complex biochemical mechanisms underlying the tumor cell transformation represent a major obstacle to the development of an ideal therapy for cancer, which is characterized by high efficacy with low side effects [1]. Nanotechnology has changed the cancer treatment scenario. In recent decades, several inorganic materials, such as calcium phosphate, gold, carbon materials, silicon oxide, iron oxide and layered double hydroxides (LDHs), have been studied for targeted drug administration [2–10]. Drug delivery via LDHs showed great in vitro and in vivo potential for the administration of bioactive molecules to cells. Recent observations showed that LDH is more biocompatible than other commonly used nanoparticles. Several pharmacologically active molecules were associated with the surface or intercalated in LDH through co-precipitation, anionic exchange reactions or other methods [11,12]. Furthermore, these nanodevices were used on target cells or organs in therapeutic gene approaches [13,14].

LDHs have been intensively studied for many decades due to their intriguing physicochemical properties. LDHs are also widely referred to as hydrotalcite-like compounds (HTlc) due to their structural similarities to hydrotalcite, which is a mineral with the formula $\text{Mg}_6\text{Al}_2(\text{OH})_{16}\text{CO}_3\cdot4\text{H}_2\text{O}$. They belong to the group of anionic clays, which are composed of divalent and trivalent metal cations that are coordinated to hydroxide anions in $\text{M(II)}(\text{OH})_6$ and $\text{M(III)}(\text{OH})_6$ edge-sharing octahedra, resulting in stacked sheets that are similar to those of brucite [15–18], as shown in Figure 1. The hydroxide layers in LDHs are positively charged due to the partial substitution of divalent metal cations by trivalent ones, and they are weakly bound to each other through the electrostatic interactions between the charged sheets and anions and by the hydrogen bonds between the hydroxides and the water molecules [19].

![Figure 1. General structure of layered double hydroxide crystal containing layers of divalent M(II) and trivalent M(III) cations arranged between two layers of hydroxides. Water and OH\(^-\) or NO\(_3^-\) anions are intercalated in the interlayer space (a), while more complex molecules or drugs can also be hosted (in this work, the garlic derivative SAMC molecule) after the anion exchange process (b).](image)

Even though it is possible to realize a great variety of LDH compounds, there are some restrictions on the substitution fraction of the divalent metal cation, namely, the $\text{M(III)}/(\text{M(II)} + \text{M(III)})$ molar fraction. Based on the evidence of experiments [20], this quantity has to be between 0.20 and 0.40; otherwise, it results in significant difficulty obtaining a pure hydrotalcite phase and avoiding the formation of other phases. LDHs are very versatile for different technological applications, in particular biological and chemical ones [21], primarily due to their layered structure, which allows for hosting even complex organic molecules, such as drugs and biomolecules, that are intercalated in the large interlayer space with wide flexibility regarding the composition and functionalization [22–26]. Moreover, there is currently an increasing interest in LDHs due to their properties as heterogeneous catalysts and supports for molecular catalysts [29–31] or photocatalysis [32], for fabrication of superhydrophobic surfaces [33,34], water treatment
and remediation [35–37] and ion-exchanger membranes [38,39]. Interestingly, anion conductivity in LDHs can be modulated by incorporating different anions in the interlayer space, allowing for their use as sensors [40–44] or as fillers in different electrochemical applications, such as fuel cells, supercapacitors and water splitting [45–47].

Different types of LDH compounds and LDH-based nanocomposites and hybrids have been made available by several synthesis methods, including exfoliation or top-down methods, as well as several chemical or mechanical methods (see, for instance, [48,49]). It was demonstrated that owing to their advantages, such as their low cost, the versatility of their chemical composition, the easy tunability of physicochemical properties, a wide range of preparation variables, unique anion exchange and intercalation properties, chemical stability and colloidal behavior, LDHs can be effectively used as nanoscale vehicles in drug delivery [11,50,51]. In particular, LDHs possess good biocompatibility, high drug-loading density, high drug-transportation efficiency and low toxicity to target cells or organs, as well as offer excellent protection to loaded molecules from undesired enzymatic degradation [49,52]. Furthermore, the intercalation of organosulfur compounds L-cysteine and L-cysteine in MgAl-LDHs by co-precipitation and ion exchange methods was demonstrated in a previous study [53].

In this work, we report on ZnAl-LDH (hereafter LDH) that was synthesized using a urea method for drug delivery of S-allyl-mercapto-cysteine (SAMC), which is a component of garlic, as well as other garlic-derived and organosulfur compounds, such as L-cysteine, DADS, SAC and L-cystine, which have been studied over the years. Their molecular structures are shown in Figure 2 [54–56]. SAMC is well-known for its anti-tumor properties, as demonstrated by many recently reported both in vitro and in vivo studies [57–62]. Experimental carcinogenesis studies indicate that the components of garlic (e.g., allyl sulfides) inhibit both the initiation and promotion stages of tumorigenesis for various types of cancer, including colorectal, lung and skin cancers. The garlic derivative SAMC can inhibit the growth of cancer cells by directly binding to sulfhydryl residues in tubulin and thereby disrupt microtubule structures in the cytoplasm of interphase cells and the spindle apparatus of mitotic cells [59]. Furthermore, SAMC is able to stop the cell cycle, preventing progression from phase G2 to phase M, which inhibits the protein kinases involved in signal transduction, blocks the opening of calcium channels and, finally, modifies the reactivity of steroid hormones with cancer cells [60].

Figure 2. Molecular structures of garlic-derived and other organosulfur compounds: L-cysteine, DADS, SAC, L-cystine and SAMC.

2. Materials and Methods
2.1. Materials

All purchased reagents were used without further purification. SAMC was kindly granted by the Wakunaga Pharmaceutical Company, Ltd. (Tokyo, Japan). SAMC was assayed in the culture media by means of a fluorimetric kit (ab211099-ABCAM Discov-
ery Drive, Cambridge Biomedical Campus, Cambridge, UK). LDH was synthesized by using Zn(NO$_3$)$_2$·6H$_2$O and Al(NO$_3$)$_3$·9H$_2$O, which were purchased from Fluka-Honeywell (Seelze, Germany) and Alfa Aesar (Thermo Fisher Scientific Chemicals, Inc., Ward Hill, MA, USA), respectively. The urea compound was purchased from Sigma Aldrich (Merk Life Science, Milan, Italy). In vitro release studies were carried out in Dulbecco’s Phosphate Buffered Saline 10X D-PBS (Euroclone S.p.A.). Deionized water was obtained via a reverse osmosis process that was carried out using the Milli Q system (Millipore, Roma, Italia). All the other reagents and solvents were characterized by the highest value of purity.

2.2. Synthesis of LDH

Micrometric LDHs with the formula [Zn$_{0.67}$Al$_{0.33}$(OH)$_2$](NO$_3$)$_{0.33}$·0.6H$_2$O (LDH-NO$_3$) were synthesized as reported in the literature [63]: 1.0 M solution of Zn(II) and Al(III), with a molar fraction Al(III)/(Al(III) + Zn(II)) = 0.33, was prepared by dissolving Zn(NO$_3$)$_2$·6H$_2$O (41.65 g, 0.14 mol) and Al(NO$_3$)$_3$·9H$_2$O (26.26 g, 0.07 mol) in 200 mL of decarbonated water. Finally, 0.42 mol of solid urea was added to this solution in order to have a urea/Al molar ratio value of 6. The obtained solution was heated under stirring and N$_2$ flux for 24 h at 100 °C. The resulting material was recovered via centrifugation, washed several times with degassed water and dried at 65 °C in an oven. The mass of the obtained material was 22.2 g, with a percentage yield close to 90%.

2.3. Intercalation of S-Allyl-Mercapto-Cysteine into LDH (LDH-SAMC)

The SAMC (0.405 g, 0.0021 mol, MW = 193.3, pKa = 9.04) was dissolved in 20 mL of degassed water, and 1M NaOH solution (2.1 mL) was added in order to obtain the corresponding anionic form of SAMC at pH = 10. Finally, LDH-NO$_3$ (0.500 g, 0.0042 mol, MW = 117.99) was dispersed in the previously closed system solution and the SAMC/Al molar ratio was 1.5. This mixture was kept under magnetic stirring at room temperature (RT) for 24 h.

The resulting solid (hereafter LDH-SAMC) was filtered under vacuum and washed twice with degassed water and then dried in an oven at 65 °C for 24 h. The obtained material was stored under P$_2$O$_5$ at RT. The LDH-SAMC intercalation compound was characterized using XRD, SEM and FT-IR. The amount of the intercalated drug was determined using UV-Vis spectrophotometry and thermogravimetric analysis.

2.4. Release Study of SAMC from LDH-SAMC

The SAMC release was performed in a phosphate buffer solution (PBS) at pH 7.2. The release studies in PBS were carried out by dispersing 127 mg of LDH-SAMC in 107 mL of medium in a closed vessel under stirring. The temperature was kept constant at 37.0 ± 0.5 °C using a thermostatically controlled circulation water bath.

Withdrawals of 2 mL were done at fixed times and the same volume of fresh medium was added after each sampling. Samples were centrifuged (Sigma 3–30KS) to obtain clear supernatants, diluted when necessary, then were analyzed using UV spectrophotometry (Agilent 8453) at $\lambda_{max} = 202$ nm according to the calibration curve previously determined ($y = -1.5398 \times 10^{-5} + 1.7899 \times 10^{-4} x$, $r = 0.9885$, standards from $5.2 \times 10^{-5}$ M to $1.6 \times 10^{-4}$ M). Any solid recovered after centrifugation was re-immersed in the initial dispersion. Drug release was monitored starting from shorter intervals (e.g., 15 min) to longer ones over about 13 days and the SAMC concentration was reported as an average of three determinations. The percentage released at each time was expressed as a percentage of the total amount of SAMC.

At the end of the release experiment, the solid was recovered via centrifugation, dried and analyzed using X-ray powder diffraction.

2.5. Characterization

X-ray powder diffraction (XRD) patterns were collected using a PanalyticalX’Pert PRO diffractometer and a PW3050/60 goniometer equipped with an X’Celerator detector,
a CuKα radiation source, a 2θ step size of 0.033° and a step scan of 50 s. The LFF ceramic tube was operated at 40 kV and 40 mA. To minimize the preferred orientation, the powder samples were carefully side-loaded onto a glass sample holder and rectangle-shaped film stripes were loaded onto an aluminum sample holder.

Thermogravimetric analysis (TGA) was carried out using a thermoanalyzer (TG-DTA Netzsch STA 490) at a heating rate of 10 °C/min with a 30 mL/min airflow.

The morphologies of the LDH and LDH-SAMC samples were investigated by means of scanning electron microscopy (SEM) secondary electron images that were taken in a field emission SEM (FESEM, model LEO SUPRA 1250, Oberkochen, Germany). In order to prevent possible charging effects during imaging, all samples were covered with a thin gold layer (approximately 5 nm). Images were collected using a 5 kV accelerated electron beam.

FT-IR (Fourier-transform infrared) spectra were measured by means of an Agilent 660 spectrometer. Each sample was dissolved in KBr powder in a weight ratio of ~1:100 and compacted in a self-standing specimen. The pellets were measured in transmission mode between 400 and 6000 cm⁻¹ using a ceramic source, a KBr beam splitter and a DTGS detector.

The amount of SAMC in the sample was determined using UV-Vis spectrophotometry (Agilent 8453) at λmax = 202 nm.

2.6. Cell Cultures

Human hepatocarcinoma (HepG2) cells were purchased from the European Collection of Cell Cultures (Promochem, Beirut, Lebanon); grown in glutamine-containing RPMI 1640 medium (Sigma, St. Louis, MO, USA) that was supplemented with 1% sodium pyruvate, 1% non-essential amino acids and 10% fetal calf serum (FCS); and incubated at 37 °C in an atmosphere of 5% CO2 in the air. Cells were routinely trypsinized and plated at a density of 4 × 10⁴ cells/cm².

2.7. Cellular Treatments

LDH-SAMC suspensions were kept at room temperature just before use and added to the cell medium at concentrations of 0.1, 0.5 and 1% (v/v). These solutions correspond to a final concentration of SAMC on the cell medium ranging from 5 to 50 µM. In parallel, as a control, the data were compared with cultures in the presence of SAMC alone at the same concentrations. The optimal concentration of SAMC was chosen and showed a sufficiently cytostatic and less toxic effect on the cells (data not shown).

2.8. Analysis of Cell Viability (Cytotoxicity)

Cell viability was assessed by staining the cells with Trypan Blue 0.4% (Sigma) according to the protocol described by W. Strober [64]. For cell viability analysis, cultures were treated with an LDH-SAMC suspension at concentrations of 0.1, 0.5 and 1% (v/v) or with a solution of SAMC at a final concentration ranging from 5 to 50 µM. After the treatment times, specifically 24 and 48 h, the culture medium was recovered and the cells were washed twice with 2 mL of PBS. They were then detached from the flask by the addition of 1 mL of trypsin/EDTA (ethylenediaminetetraacetic acid) by Biowest and recovered for further analysis. To ensure that all cells were retrieved from the flask, an additional wash in PBS was performed. Subsequently, 50–100 µL of cell suspension was added to 50–100 µL of Trypan Blue; after 5 min of incubation at room temperature, viable cells were loaded and counted using a Burker chamber under a phase-contrast light microscope.

2.9. Cell Migration Assay Using the Scratch Test

The ability of HepG2 cells, untreated or treated with either LDH-SAMC or SAMC alone, to reform a monolayer at 100% confluence after mechanical shear was evaluated using the “scratch test” method [65]. Scratching involves a longitudinal surface incision at the plate diameter, which generates a directional migratory response. HepG2 cells were expanded in 75 cm² flasks until approximately 90% confluence was reached. After being
removed from the medium, cells were washed 2 times with 2 mL of PBS, then detached via the addition of 1 mL of trypsin/EDTA, incubated for 5 min at 37 °C and 5% CO₂, resuspended in 9 mL of complete medium and finally harvested in a 50 mL Falcon tube. Subsequently, they were seeded in a 6-well plate (3–3.5 mL of cell suspension per well) and incubated with 0.1, 0.5 and 1% (v/v) LDH-SAMC suspensions or SAMC at a final concentration of 5, 25 or 50 µM for 24 h at 37 °C and 5% CO₂ to allow the formation of a complete monolayer. Once the confluence was reached, the medium was removed and the incision was made with a spatula that was previously treated with ethyl alcohol. After removing the debris produced as a result of cutting, the monolayer of HepG2 cells was washed 3 times with PBS and maintained in the presence of a culture medium. The incision areas were visualized under a microscope after 48 h of incubation. Cell migration and the effect of treatments on sulcus closure were assessed as the number of cells that migrated within the sulcus itself over 48 h via image acquisition and analysis using “Image J” software (ImageJ bundled with 64-bit Java 1.8.0_172). Data were expressed as the percentage migration compared to the control placed at 100%.

3. Results and Discussion
3.1. Preparation and Characterization of LDH-SAMC

Since nitrate anions are easier to exchange in comparison with carbonate or chloride anions, LDH in nitrate form was chosen as the starting material to intercalate SAMC anions. The intercalation of the SAMC in anionic form occurred via an ion-exchange reaction in agreement with the following reaction:

\[
\text{LDH-NO}_3 + \text{SAMC}^- \rightarrow \text{LDH-SAMC} + \text{NO}_3^-
\]

The XRD patterns of LDH-NO₃ and LDH–SAMC are shown in Figure 3. LDH-NO₃ was well crystallized and the peak at 8.9° of 2θ was related to the presence of the pure nitrate form. After intercalation, the (003) reflection was shifted to lower 2θ values corresponding to 13.9 Å, which confirmed the successful intercalation of SAMC⁻ anions. The absence of the peaks belonging to the pristine phase suggested that the nitrate anions that were not exchanged by SAMC (see the chemical composition reported below) were solubilized in the SAMC phase with the formation of a solid solution. A loss of crystallinity upon intercalation, probably due to stacking disorder, was observed, as confirmed via a general broadening of the peaks.

![Figure 3. XRD patterns of LDH-NO₃ (a) and LDH-SAMC (b).](image)

The chemical composition of the intercalation compound was investigated by combining the thermal analysis (TGA) and UV measurements. Moreover, the TGA allowed for studying the thermal stability of LDH-SAMC. The TGA curves for LDH-NO₃ and LDH-SAMC are shown in Figure 4. LDH-NO₃ displayed a first weight loss of 8.4% up to 170 °C, which was due to the loss of intercalated water molecules. Then, a second weight loss up to 600 °C was observed, which was compatible with the loss of nitrate from the interlayer region and water coming from the layer dehydroxylation with the formation of ZnO and...
The TGA of LDH-SAMC showed three weight losses: the first, from 70 to 170 °C, was related to the hydration water; the second, until 600 °C, was due to the loss of residual nitrates, layer dehydroxylation and decomposition of SAMC; the third could be ascribable to the decomposition of ZnSO₄ that was formed upon the SAMC decomposition. Finally, it was possible to assign to LDH-SAMC the following formula:

\[ [\text{Zn}_{0.67}\text{Al}_{0.33}(\text{OH})_2]\text{SAMC}_{0.15}(\text{NO}_3)_{0.18}\cdot 0.6\text{H}_2\text{O} \]

The FT-IR spectra of the pristine LDH-NO₃ precursor, neat SAMC and LDH-SAMC are displayed in Figure 5 (a, b, c), respectively. The FT-IR spectrum of the LDH pristine precursor (Figure 5 (a)) showed the characteristic features that are widely reported for LDH-NO₃. Briefly, the O-H stretching vibration in the brucite-like layers and the hydration water molecules produced a broad band in the 3000–3800 cm⁻¹ range, centered at approximately 3480 cm⁻¹ [66,67], whose broadening is typically attributed to hydrogen bonds formed between the hydroxides and the hydration water molecules [68]. The band observed near 1617 cm⁻¹ was assigned to the bending vibration of the interlayer water molecules [69]. A strong absorption band at about 1384 cm⁻¹ arose from the ν₃ stretching vibrations of free interlayer nitrate anions with D₃h symmetry, as confirmed by the presence of bands at 1762 and 834 cm⁻¹ [70]. The narrow peak at 1050 cm⁻¹ could be assigned to the intercalated NO₃⁻ as well [71]. The bands in the low-frequency region were due to the lattice vibrations, i.e., to all of the metal–hydroxide stretching and bending modes [69,72]. In particular, the narrow band at about 427 cm⁻¹ arose from metal-oxygen bond M-O-M vibrations in the brucite-like layer [66], and the broader band at approximately 608 cm⁻¹ was attributed to the lattice vibration modes that are relevant to the Zn-OH translation lattice modes [69].

The FT-IR spectrum of neat SAMC (Figure 5 (b)) was similar to those of L-cysteine [56,73], S-allylcysteine (SAC) [56], diallyl disulphide (DADS) [54] and L-cystine [55] due to the identical functional groups in their respective molecular structures (see Figure 1). The SAMC spectrum was also compared with the standard assignments of functional groups [74]. A shoulder at approximately 3429 cm⁻¹ was consistent with the amine N-H stretch [55].
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metric -NH3+ deformation. Interestingly, similarly to L-cysteine [55], these assignments made it reasonable to also suppose a zwitterionic nature for SAMC in the solid state. Peaks due to C-C stretching vibrations occurred in the fingerprint region below 1300 cm⁻¹, whose peaks corresponded to those of the functional groups in the SAMC molecule. In particular, the contributions from C-C stretching vibrations around 1100 cm⁻¹, C-H deformation at 993 cm⁻¹ and C-S stretching vibration in the region 700–600 cm⁻¹ could be clearly observed. Characteristic peaks due to C-H stretching vibrations in the range of 2800–2950 cm⁻¹ also appeared in the LDH-SAMC spectrum. After the SAMC intercalation in the LDH interlayer galleries, the 1500–1350 cm⁻¹ region in the FT-IR spectrum (see Figure 5 (c)) was dominated by absorptions due to COO⁻ asymmetric (1587 cm⁻¹) and symmetric (1399 cm⁻¹) stretching, which overlapped those that were assigned to the bending vibration of the interlayer water and stretching of the residual NO3⁻ groups, respectively. The presence of NO3⁻ was in agreement with the chemical composition that was obtained using UV and TGA. Interestingly, the intense absorption at 1490 cm⁻¹ that was found in the SAMC spectrum (Figure 5 (b)) and tentatively

Figure 5. FT-IR spectra of the (a) pristine LDH-NO3 precursor, (b) neat SAMC crystal, and (c) LDH-SAMC. The dotted line corresponds to the pristine LDH-NO3 precursor for comparison purposes.
assigned to NH$_3^+$ group was not present in the FT-IR spectrum of LDH-SAMC that was found according to the intercalation procedure performed at pH 10 in which SAMC was mainly present in anionic form. These results also confirm that after the ion exchange, SAMC into LDH preserved its functionality and structure. Such capability of LDHs was already reported for intercalation of other drug molecules [76–79], including L-cystine and L-cysteine [53].

The morphological features of the LDH-SAMC were investigated using FE-SEM and compared with the pristine components, i.e., SAMC and LDH-NO$_3$ (Figure 6). The SAMC crystals exhibited a flaky morphology with a smooth surface and large micrometer-sized aggregates consisting of an almost flat stacking of elongated hexagonal flakes (Figure 6a). The FE-SEM micrograph of pristine LDH-NO$_3$ revealed the typical aggregation of clusters of small randomly oriented hexagonal-like platelets [80,81]. The diameter of LDH-NO$_3$ crystallites, as estimated from the FE-SEM image of Figure 6b, was about 3 µm. Furthermore, as shown in Figure 6c, LDH-SAMC exhibited roughly the same morphological features of the pristine LDH precursor with thin hexagonal-like platelets. However, more irregular sizes and shapes of the flake-like crystals could be clearly observed, as well as an overall finer structure with a reduction in the average crystallite size to about 2 µm. It is worth pointing out that the roughly identical morphology of LDH-NO$_3$ and LDH-SAMC, which was completely different from that of SAMC (see Figure 6a), clearly indicated that both the metal hydroxide sheets and the plate-like geometry of the LDH precursors were preserved during the anion exchange modification, as confirmed by the XRD results. Moreover, the broadening of the XRD reflections in the LDH-SAMC spectrum that is reported in Figure 3 well supported the loss of crystallinity due to the crystallite size reduction.

Figure 6. FE-SEM images of (a) SAMC alone, (b) pristine LDH-NO$_3$ and (c) LDH-SAMC.

3.2. SAMC Release Studies from LDH-SAMC

An in vitro drug release study, reported in Figure 7, was performed in a phosphate buffer solution at pH 7.2 and 37 °C. The SAMC release from LDH-SAMC was initially characterized by a clear burst effect in the first four hours, during which, 32% of the SAMC was released. This fact may be explained by the liberation of SAMC anions that were immobilized on the surface of the nanocrystals and those intercalated at the edges of the interlayer regions. Subsequently, the percentage release increased at a slower rate, reaching 42% after 48 h. Once the 48 h had elapsed, the percentage stabilized at 43% and remained constant for the entire period of the investigation.
Figure 7. Release curve of SAMC from the LDH-SAMC. Operative conditions: phosphate buffer medium at pH 7.2.

The solid recovered from the release experiments was characterized using XRD. Since the total release was lower than 40%, the pattern of the recovered LDH-SAMC, shown in Figure 8, displayed a reflection corresponding to 14.7 Å, which very likely belonged to the SAMC phase. This interlayer distance suggested that the anions of the phosphate buffer solution, both as hydrogen phosphates and dihydrogenphosphates, were mainly present on the LDH surface and intercalated in the SAMC phase.

Figure 8. XRD pattern of the LDH-SAMC that was recovered after the release studies.

3.3. Cytotoxicity of the LDH-SAMC and SAMC Treatments

The cytotoxicity of the treatments was assessed using the Trypan Blue exclusion test (see the Materials and Methods section). The HepG2 cells were treated for 48 h in the presence of different concentrations of the SAMC loaded in the LDH (Figure 9a) or SAMC alone (Figure 9b). As can be seen in Figure 9a, the LDH-SAMC suspension showed similar levels of cytotoxicity to those subjected to the SAMC treatment alone, where the percentage of cytotoxicity after 48 h of incubation ranged from 15.4 to 18.5%. In contrast, the HepG2 cellular samples, treated with LDH suspension for 48 h, showed negligible cytotoxicity (Figure 9a). The percentages of cytotoxicity, shown in the figures, represent the mean ± the standard deviation (SD) of two independent experiments, with each experiment carried out in triplicate; therefore, the total number of replicas was six ($n = 6$). In conclusion, as expected, the HepG2 cells showed low cytotoxicity after 48 h of incubation, both in the presence of the LDH-SAMC components and in the SAMC treatments.
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3.4. Treatment of HepG2 Cells with the LDH-SAMC Complex Enhanced the Inhibition of Tumor Migration

To characterize the efficacy of SAMC delivery via the intercalation in LDH, tumor cell migration was assessed by scratch test (Figure 10) and compared by culturing HepG2 cells in the presence of different concentrations of the drug loaded inside the LDH (Figure 11a) or alone (Figure 11b). The graph in Figure 11a shows a clear improvement in the inhibition of the migratory capacity of HepG2 cells when SAMC was delivered by LDH. In fact, after 48 h of incubation in the presence of LDH-SAMC at 1.0%, the reduction in the migration reached 90% (Figure 11a) compared to the control set at 100. SAMC alone, at 50 µM concentrations, could reduce the migration by 70% (Figure 11b).

![Figure 9](image1.png)

**Figure 9.** Percentage of cytotoxicity of the HepG2 cells after 48 h of treatment with the suspension of pristine LDH and LDH-SAMC (a) and SAMC alone (b) at several concentrations. Values represent the mean ± SD of 2 independent experiments ($n = 6$) (Student’s t-test; * $p < 0.01$ compared to the control).

![Figure 10](image2.png)

**Figure 10.** Results from the scratch test. The migration of HepG2 cells was significantly reduced by treating the cells for 48 h with the LDH-SAMC preparation (a) in proportion to the increasing concentration from 0.1 to 1.0% in the culture medium. Treatment with the SAMC molecule alone (b), symbolized by garlic, showed a similar effect, reducing the cell migration in proportion to the concentration set from 5 to 50 µM, but less than that observed in the presence of the LDH-SAMC component.
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Figure 11.

4. Conclusions

In this work, the synthesis and characterization of a new intercalation compound LDH-SAMC for drug delivery of garlic derivative S-allyl-mercapto-cysteine (SAMC), which is
well-known for its anti-tumor properties, is reported. The LDH-SAMC intercalation compound, with the following formula [Zn$_{0.67}$Al$_{0.33}$(OH)$_2$]SAMC$_{0.15}$[NO$_3$]$_{0.18}$·0.6H$_2$O, was characterized using different techniques, including X-ray powder diffraction, SEM and FT-IR. The resulting data suggested the effective intercalation of the molecule in the layered structure, as confirmed by the (003) reflection in the XRD spectrum for LDH-SAMC, which was shifted to lower 2θ values (corresponding to an interlay distance of 13.9 Å). Finally, its release properties in a phosphate buffer medium were determined. A loss of crystallinity upon intercalation, probably due to stacking disorder, was observed and confirmed using a general broadening of the peaks. LDH-SAMC exhibited roughly the same morphological features of pristine LDH precursors in the SEM image. However, more irregular sizes and shapes of the flake-like crystals could be clearly observed, as well as an overall finer structure, with a reduction in the average crystallite size to about 2 µm. The FT-IR spectrum of LDH-SAMC exhibited a richly structured spectrum in the fingerprint region below 1300 cm$^{-1}$, whose peaks corresponded to those of functional groups in the SAMC molecule. In vitro drug release studies were performed in a phosphate buffer solution at pH 7.2 and 37 °C and analyzed using UV spectrophotometry. The SAMC release from the compound was initially characterized by a quick release until 32% in the first four hours, followed by a slow increase until 42% after 48 h, and the percentage stabilized and remained constant for the entire period of investigation at around 43%. The solid recovered from the release experiments was characterized using XRD. Since the total release was lower than 40%, the first peak at 14.7 Å very likely belonged to the intercalated form of the LDH with SAMC. The LDH-SAMC complex that was developed in this study offers a very promising approach for the delivery of SAMC to cancer cells.

In conclusion, the preliminary results of the present study highlighted the possibility of improving the response of an anticancer drug [82] via its delivery through LDH particles. This approach was found to be safe and efficient in reducing some of the typical invasive features of a very aggressive tumor, such as human hepatoma. Obviously, the observations made in vitro need subsequent in vivo experimentation, with all its possible limitations. To this end, several in vitro and in vivo studies on this promising therapeutic approach are ongoing in our laboratory.

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